

*Research article*

## **Citrate coated iron oxide nanoparticles: Synthesis, characterization, and performance in protein adsorption**

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**Abstract:** Magnetic nanoparticles (MNPs) are extensively utilized in biomedicine as part of controlled drug release systems, hyperthermia, and magnetic resonance imaging. Surface modification of MNPs not only enhances their stability and biocompatibility but also increases affinity with certain molecules, allowing them to be used in protein separation and adsorption processes. This article reports the synthesis and characterization of iron oxide MNPs functionalized with citric acid (IONPs@CA) to evaluate their performance in protein adsorption. The nanoparticles were characterized using various techniques such as transmission electron microscopy (TEM), X-ray diffraction (XRD), dynamic light scattering (DLS), thermogravimetric analysis (TGA), and Fourier-transform infrared spectroscopy (FT-IR). The percentage of lysozyme (Lyz) adsorbed by IONPs@CA was 84.9%, while the IONPs sample only adsorbed 5.9%. In silico evaluation results showed some repulsion bonds obtained in Lyz-IONPs and hydrogen bonds, carbon-hydrogen bonds, and van der Waals interactions in Lyz-IONPs@CA. These results may be novel since no previous research was found specifying this type of interaction between lysozyme and IONPs and/or IONPs@CA. The maximum adsorption efficiency obtained for the coated nanoparticles was 88.3%.

**Keywords:** iron oxide nanoparticles; citric acid functionalization; protein purification; in silico study

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**Abbreviations:** ASN: Asparagine; ATR-FT-IR: Attenuated total reflection Fourier-transform infrared spectroscopy; DLS: Dynamic light scattering; GLU: Glutamine; ILE: Isoleucine; IONPs: Iron oxide nanoparticles; IONPs@CA: Citric acid coated iron oxide nanoparticles; LYS: Lysine; Lyz: Lysozyme; MNP: Magnetic nanoparticles; PDB: Protein database; RCSB: Research Collaboratory for Structural Bioinformatics; SER: Serine; TEM: Transmission electron microscopy; TGA: Thermogravimetric analysis; TRP: Tryptophan; UCSF: University of California, San Francisco; VAL: Valine; XRD: X-ray diffraction

## 1. Introduction

Protein purification processes are widely employed in various biotechnology areas, aiming primarily to separate proteins from the complex mixtures in which they are naturally present. Purification is crucial when structurally and functionally characterizing proteins of interest. Ultrafiltration [1], electrophoretic separation [2], precipitation [3], and chromatography [4] are among the most used techniques for protein isolation. Chromatography, particularly affinity chromatography, is favored by researchers due to its high selectivity [5]. In affinity chromatography, separation occurs due to the various interactions that a protein can have with specific ligands. Antigen–antibody binding and recognition between an enzyme and its substrate are among these interactions [6]. Peptides [7,8], synthetic oligonucleotides [9,10], metal ions [11–14], and antibodies [15] are among the most used affinity ligands for protein isolation. However, these processes have limitations such as time consumption and the need for expensive instrumentation [16,17].

Magnetic separation emerges as an alternative to conventional procedures due to its easy implementation and few steps, which can be carried out in one or two vials at most. Other advantages include the ability to work directly with crude samples without prior treatment [18] and maintaining protein integrity after purification [19]. Magnetic carriers with immobilized ligands on their surface are used for separation. These carriers are added to the desired mixture to achieve protein binding and, subsequently, the entire complex can be isolated using an external magnetic field [20].

Magnetic nanoparticles (MNPs), mainly magnetite ( $\text{Fe}_3\text{O}_4$ ) and maghemite ( $\gamma\text{-Fe}_2\text{O}_3$ ), are the most used magnetic carriers in recent years. Properties such as rapid response to a magnetic field, large surface area, and mechanical stability make MNPs attractive for magnetic separation [21]. Their nanoscale size gives them superparamagnetic properties, meaning they exhibit no residual magnetization once the external magnetic field is removed [22]. However, their use in biotechnology depends heavily on their colloidal stability. Therefore, most authors reporting MNP applications in biotechnology work with MNPs coated with stabilizing agents, which not only improve colloidal stability but also enhance biocompatibility and reduce nanoparticle toxicity [23–26].

In recent years, several researchers have utilized magnetic materials for protein purification and/or immobilization (e.g., antibodies and enzymes). Zeng et al. (2020) developed Ni(II)-chelated  $\text{Fe}_3\text{O}_4$  nanoparticles to immobilize proteins tagged with polyhistidine [27]. They found that the nanoparticles could be reused up to six times without affecting the activity of the immobilized protein. Lodhi et al. (2022) reported an innovative affinity purification method for exopolygalacturonase (Exo-PG) using  $\text{Fe}_2\text{O}_3$  magnetic nanoparticles superficially modified with galacturonic acid [28]. Tavakoli et al. (2019) synthesized mesoporous silica-coated magnetic nanoparticles for recombinant protein separation, achieving a maximum adsorption capacity of 235.21  $\mu\text{g}$  of protein per milligram of nanoparticles [29].

Most of these studies are based on affinity principles, utilizing polymeric molecules or, in some cases, double functionalization of nanoparticles to enhance protein adsorption. This work proposes a simpler method for Lyz adsorption onto iron oxide nanoparticles through citrate functionalization. This coating can enhance the interaction between nanoparticles and proteins, facilitating their immobilization.

## 2. Materials and methods

### 2.1. Materials

Ferric chloride hexahydrate ( $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$ ,  $\geq 98\%$ ), anhydrous citric acid [ $\text{HOC}(\text{COOH})(\text{CH}_2\text{COOH})_2$ ,  $99\%$ ], ferrous chloride tetrahydrate ( $\text{FeCl}_2 \cdot 4\text{H}_2\text{O}$ ,  $99\%$ ), dibasic sodium phosphate ( $\text{Na}_2\text{HPO}_4$ , ACS  $\geq 99\%$ ), monobasic potassium phosphate ( $\text{KH}_2\text{PO}_4$ , suitable for cell culture,  $\geq 99\%$ ), and chicken egg lysozyme (Lyz,  $\geq 90\%$ ) were sourced from Sigma-Aldrich. Hydrochloric acid (HCl, PA) and sodium hydroxide (NaOH, a.c.s) were obtained from Fermont.

### 2.2. Synthesis of iron oxide nanoparticles and subsequent citric acid coating

Iron oxide nanoparticles (IONPs) were synthesized following the procedure described by Medina-Espinosa (2021) with some modifications. A solution of NaOH (0.9 mol/L) was prepared, to which a mixture of  $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$  (1.28 mol/L),  $\text{FeCl}_2 \cdot 4\text{H}_2\text{O}$  (0.64 mol/L), and HCl (0.4 mol/L) [30] was added dropwise using a peristaltic pump at 48 rpm. The reaction mixture was kept in an ultrasonic bath under a nitrogen atmosphere and mechanical agitation (450 rpm) for 30 min at room temperature. After completion of the reaction, the pH of the mixture was approximately 12. The product was collected using a neodymium magnet, washed three times with distilled water, and vacuum dried.

Subsequently, 250 mg of nanoparticles were re-dispersed in 200 mL of deionized water, and the pH was adjusted to 10. Then, 1 mL of an aqueous solution of citric acid (0.25 g/mL) was added, and the mixture was mechanically stirred for 6 h [31]. After this time, the citric acid-coated nanoparticles (IONPs@CA) were collected magnetically, washed with deionized water, and vacuum-dried. Characterization techniques (specifically, FT-IR, DLS, and TGA) showed indications of the presence of coating on the surface of the nanoparticles. Details of these results are discussed below.

### 2.3. Characterization of nanoparticles

Both IONPs and IONPs@CA were analyzed using different characterization techniques. XRD was performed using a Bruker diffractometer (Bruker, D8 Advance, Germany). The diffraction patterns were recorded using  $\text{Cu-K}\alpha$  ( $\lambda = 1.54183 \text{ \AA}$ ) as incident radiation, in a range of  $10\text{--}90^\circ$ , with an increment of  $0.02^\circ$ ; the counting speed was set to 10 s per point. ATR-FT-IR was carried out on a PerkinElmer spectrometer (PerkinElmer, FRONTIER, USA); spectra were acquired in the range of  $400\text{--}4000 \text{ cm}^{-1}$ . The morphology and size of the nanoparticles were determined using TEM. Images were obtained on a JEOL microscope (JEOL, JEM-2100, Japan); for this, a sample of nanoparticles was sonicated in 2-propanol, deposited on a carbon-copper grid, and allowed to dry overnight. TGA was conducted using a Netzsch thermogravimetric analyzer (Netzsch, STA 409 PC Luxx, Germany). During this analysis, samples were heated to  $900 \text{ }^\circ\text{C}$  at a rate of  $20 \text{ }^\circ\text{C}/\text{min}$  under an inert argon atmosphere. The hydrodynamic diameter and zeta potential of the nanoparticles were determined by

DLS using a Zetasizer Nano sampler (Malvern Instruments, Zetasizer Nano ZS, UK) equipped with a He-Ne laser ( $\lambda = 633$  nm). Hydrodynamic diameter measurement of the nanoparticles was performed at 25 °C in a range of 0.3–10  $\mu\text{m}$  using polystyrene cuvettes. Samples were at a concentration of 0.1% (w/v), and water was used as the dispersing medium. Zeta potential determination was carried out using 0.1 M phosphate buffer (pH 7.4). Protein quantification was performed according to the Bradford method [32] using a Thermo Scientific microplate reader (Thermo Scientific, Multiskan GO, USA).

#### 2.4. Protein adsorption

The adsorption assay was conducted following the method reported by Rahman et al. (2012) with some modifications. A Lyz solution ( $1.5 \times 10^{-5}$  mol/L) in 0.1 mol/L phosphate buffer (pH 7.4) was prepared. Both nanoparticle samples (IONPs and IONPs@CA) were used for the adsorption experiment. Approximately 5 mg of nanoparticles were added to 5 mL of the working solution, and the mixture was mechanically stirred for 4 h [33]. After this time, the protein content in the supernatant was determined using the Bradford assay [32]. In a 96-well microplate, 100  $\mu\text{L}$  of the supernatant and 100  $\mu\text{L}$  of the Bradford reagent were added, and after 10 min of incubation, absorbance at 595 nm was read. Protein quantification was carried out using a bovine serum albumin calibration curve. The percentage of Lyz adsorbed by the nanoparticles was calculated as expressed in Eq 1:

$$\text{adsorption}\% = \frac{C_0 - C_f}{C_0} \times 100 \quad (1)$$

where  $C_0$  and  $C_f$  are the initial and final concentrations, respectively, of Lyz expressed in  $\mu\text{g}/\text{mL}$  [34].

Under these conditions, the IONPs@CA sample adsorbed the greater amount of protein; therefore, it was chosen to evaluate its maximum adsorption capacity. For this purpose, a total of seven Lyz solutions were prepared, ranging in concentrations from 5.8 to 23.6  $\mu\text{g}/\text{mL}$ . Aliquots of 1 mL from each solution were taken and placed in seven different 1.5 mL vials, each containing, approximately 1.5 mg of IONPs@CA. The mixtures were stirred for 4 h, and after this time, the remaining protein concentration in the supernatant after adsorption was determined using the Bradford method [32].

#### 2.5. In silico evaluation by molecular docking

The crystalline structure of lysozyme (PDB code: 1AT5) was obtained from the RCSB Protein Data Bank (PDB), while magnetite and citrate were obtained using simplified molecular-input line-entry system (SMILE) sequences and modeled in AutodockTools 1.5.7. AutoDock 4.2 was employed to investigate the interactions between magnetite, citrate, and lysozyme. Initially, the structures of magnetite and citrate were drawn using Avogadro, and their geometries were optimized using AutoDock 4.2. Prior to docking analysis, hydrogen atoms and water molecules were removed from the protein, and energy minimization was performed using UCSF Chimera 1.15. For the docking calculations in AutoDock 4.2, the Lamarckian genetic algorithm was utilized, with grid parameters set to  $130 \times 130 \times 130$  and a spacing of 1 Å. To determine the binding sites on lysozyme, the ligands were allowed to move within the grid region through 50 runs to explore potential binding conformations. Additionally, the docked complex structures of the ligands and the surrounding amino acid residues were analyzed using BIOVIA Discovery Studio Visualizer.

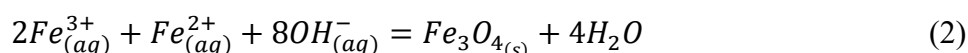
## 2.6. Statistical analysis

Experiments were conducted in triplicate and expressed as mean values and their standard deviations. A significance level of  $p \leq 0.05$  was employed for all samples. The data were analyzed using RStudio version 1.4.2.1.

## 3. Results and discussion

### 3.1. Synthesis of iron oxide nanoparticles and subsequent citric acid coating

Nanoparticles were synthesized using the coprecipitation method, resulting in a black solid (magnetite) [34]. However, the presence of atmospheric oxygen can cause the oxidation of  $Fe_3O_4$ , leading to the formation of  $\gamma-Fe_2O_3$ , which is a brown solid [35]. To prevent this phenomenon, the reaction was carried out in an inert nitrogen ( $N_2$ ) atmosphere. The reaction involved in the formation of magnetite, as the main product, is represented in Eq 2. During synthesis, in addition to classical mechanical stirring, ultrasonic agitation was employed, which may contribute to obtaining nanoparticles with homogeneous size distribution compared to those obtained through conventional coprecipitation [36]. The coating of IONPs with citric acid was carried out at pH 10 to ensure the formation of carboxylate groups on the surface of the nanoparticles, which enhance their colloidal stability [37] and facilitate protein adsorption [38].

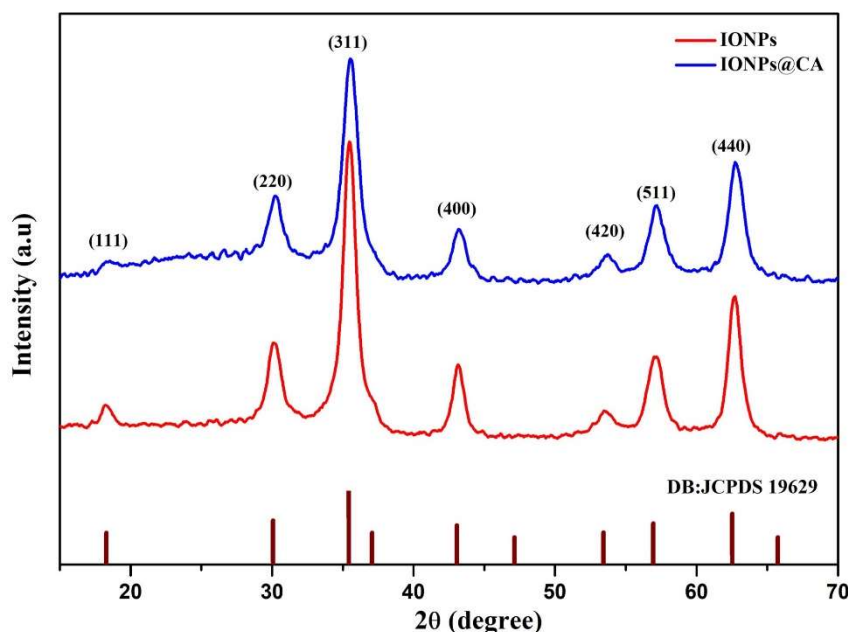


### 3.2. Characterization of nanoparticles

#### 3.2.1. X-ray diffraction (XRD)

Figure 1 shows the XRD pattern of nanoparticles with and without coating. Both patterns can be associated with the inverse spinel cubic structure of magnetite and maghemite [39]. The main peaks are observed at the following positions: 30.2, 35.6, 43.3, 53.6, 57.3, 62.9°. These peaks can be indexed to the planes (hkl) (220), (311), (400), (422), (511), and (440), respectively, according to the standard pattern of magnetite (JCPDS 19629). No differences are observed when comparing the diffraction patterns of both samples, suggesting that the coating process does not affect the crystalline structure of the nanoparticles [40]. The crystallite size and lattice parameter for each sample were estimated using High Score Plus (3.0.2) software, which utilizes Rietveld refinement for the estimations (see Figures S1 and S2 and Tables S1 and S2). The estimated crystallite size for IONPs was 7.9 and 7.6 nm for IONPs@CA. These values are lower than those generally obtained when  $NH_4OH$  is used as a base during the coprecipitation reaction [41,42]. The difference in sizes can be explained by considering that  $NaOH$  is a strong base, which promotes nucleation but affects the growth of the nuclei, resulting in a large number of small-sized particles [43]. Furthermore, the lattice parameter value obtained for IONPs was  $8.367 \pm 0.005 \text{ \AA}$ , which falls between the values for maghemite and magnetite ( $8.3515$  and  $8.3960 \text{ \AA}$ ) [44] and  $8.357 \pm 0.002 \text{ \AA}$  for IONPs@CA. The reduction in the lattice parameter of the nanoparticles after functionalization may occur due to the interaction between the coating atoms and the nanoparticle's atoms, causing the contraction in the crystal lattice [45]. Some authors also report

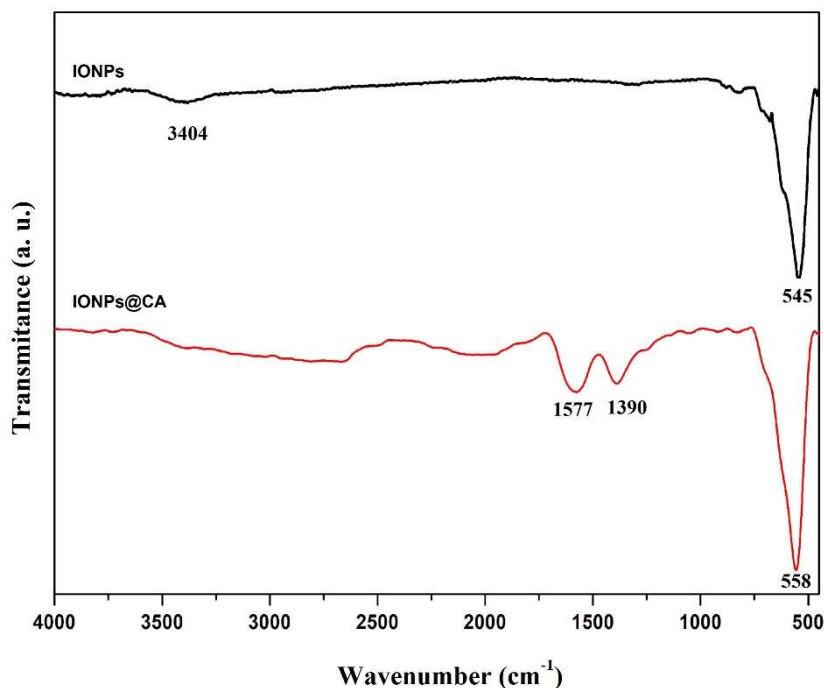
this variation in the lattice parameter of nanoparticles after functionalization [41,42]. Although the black color of the synthesized IONPs suggests the presence of  $\text{Fe}_3\text{O}_4$ , the nanometric nature of the material facilitates its oxidation to  $\gamma\text{-Fe}_2\text{O}_3$  upon exposure to atmospheric oxygen. Distinguishing between magnetite and maghemite using XRD can be challenging because both phases possess very similar crystal structures and nearly identical lattice parameters, leading to almost indistinguishable diffraction patterns; therefore, we assume that the synthesized iron oxide nanoparticles are a mixture of both phases.



**Figure 1.** XRD pattern of IONPs and IONPs@CA.

### 3.2.2. Fourier-transform infrared spectroscopy

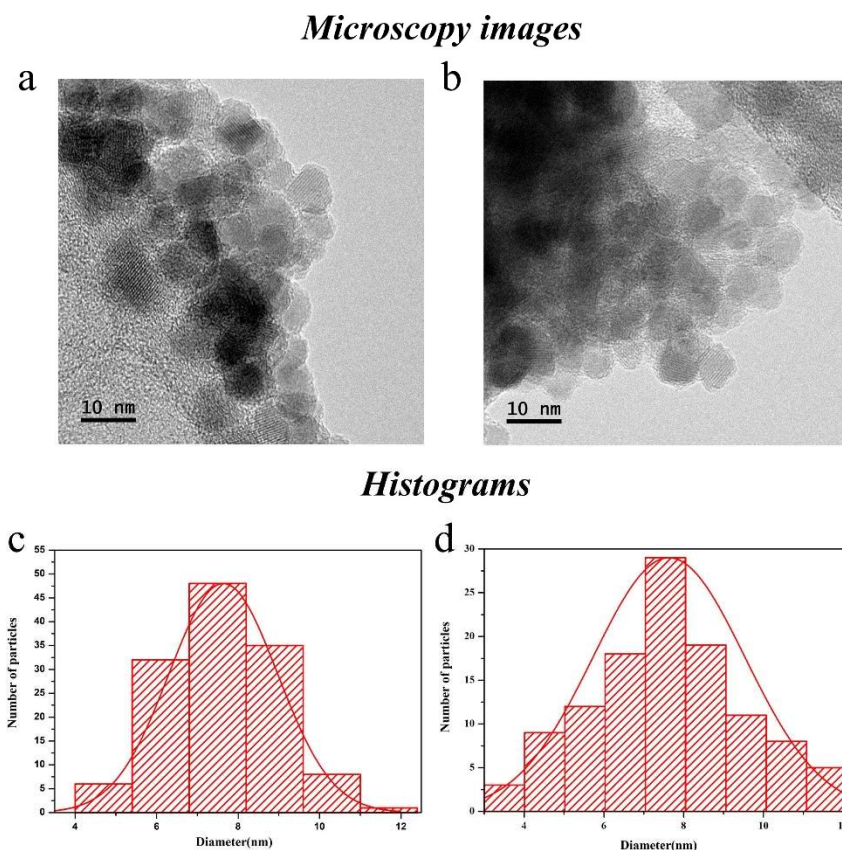
The IR spectra of IONPs and IONPs@CA samples are presented in Figure 2. For IONPs, an intense signal is observed near  $545\text{ cm}^{-1}$ , assignable to the stretching vibration of the Fe–O bond [46], thus confirming the formation of iron oxide. Near  $3404\text{ cm}^{-1}$ , a broad and weak band corresponding to the O–H group of water present on the material’s surface is observed. In the spectrum of IONPs@CA, the band near  $558\text{ cm}^{-1}$  indicates the presence of an iron oxide core as it corresponds to the Fe–O bond. The slight shift of this signal compared to IONPs can be explained by the binding of carboxylate groups to the nanoparticles, causing variations in the vibration frequencies of the bond between iron and oxygen atoms. Lastly, the bands observed near  $1577$  and  $1390\text{ cm}^{-1}$  can be attributed to the asymmetric and symmetric stretching vibrations of the carboxylate group, respectively. The presence of these signals confirms the formation of citrate coating on the surface of the nanoparticles [37,38,46,47].



**Figure 2.** FT-IR of IONPs and IONPs@CA.

### 3.2.3. Transmission electron microscopy

In Figure 3, micrographs of both samples along with the corresponding histograms are presented. The images reveal the tendency of both samples to form agglomerates. Despite this, in both images, some individual particles within the agglomerate can be distinguished, which exhibit nearly spherical morphology. Particles' average size is approximately 8 nm for both samples, making them suitable for biomedical applications [48,49]. This similarity in size between IONPs and IONPs@CA aligns with findings reported by Li et al. (2013) and Atrei et al. (2021). These authors demonstrated that the post-synthesis coating process has no significant effects on the size of the nanoparticles [50,51]. Furthermore, this value is very close to the crystallite size obtained via XRD (see Table 1) after Rietveld refinement; so, this observation could provide evidence of the formation of a monocrystalline material [41].



**Figure 3.** Microscopy images: (a) IONPs, (b) IONPs@CA. Histograms: (c) IONPs, (d) IONPs@CA.

**Table 1.** Particle size according to XRD and TEM.

Sample	Crystallite size (nm)	TEM size (nm)
IONPs	$7.9 \pm 0.2^*$	$7.58 \pm 0.06^+$
IONPs@CA	$7.6 \pm 0.5^*$	$7.56 \pm 0.11^+$

\*Estimated standard deviation (from Rietveld refinement); <sup>+</sup>standard error.

Determining the size of nanoparticles is crucial for our objectives, as this parameter significantly influences the magnetic behavior of the sample [52]. In our case, it is desirable for the nanoparticles to behave as superparamagnetic material. However, since we do not have magnetic characterization, we analyzed published works on the subject to reach a conclusion. As can be seen, both IONPs and IONPs@CA have particle sizes below 20 nm, which is considered the critical size for nanoparticles to exhibit superparamagnetic behavior [53]. There is sufficient evidence that nanoparticles with diameters below this critical value exhibit superparamagnetic properties [54–57]. On the other hand, organic coatings can also affect the magnetic behavior of nanoparticles [58]. Some authors have assessed this effect. For instance, Li et al. (2013) obtained magnetite samples coated with citric acid at different coating percentages (5.2% and 3.5%) [50]. Magnetic characterization at room temperature showed no hysteresis, which is a unique characteristic of superparamagnetic materials [59], for the

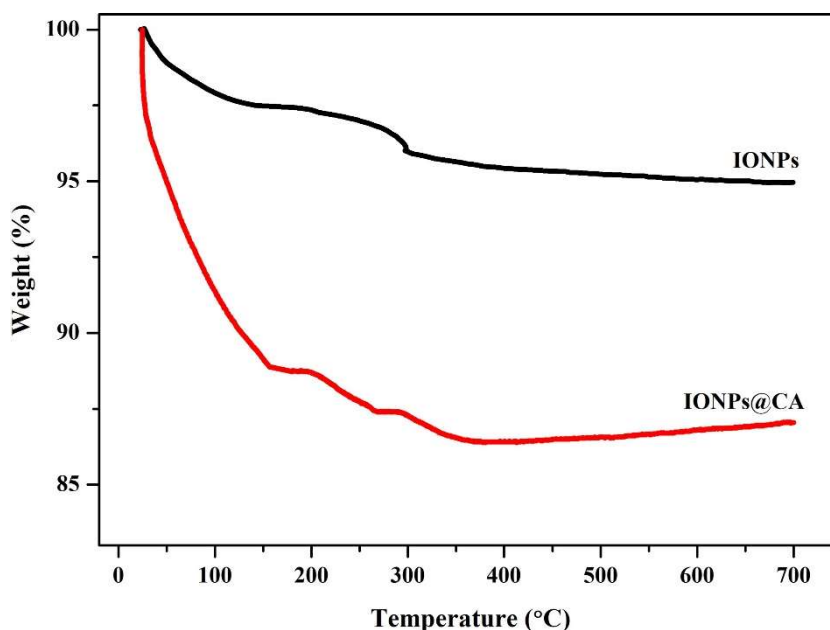


sample with 5.2% coating. Similar results have been reported by Omelyanchik et al. (2021) and Blanco-Andujar (2015) [60,61]. It is important to note that this bibliographic analysis focused on magnetic measurements conducted at room temperature, as our adsorption experiments were performed at the same temperature. Therefore, it can be assumed that the samples obtained in this work possess superparamagnetic properties, which is advantageous for our purposes; due to the absence of remanent magnetization, once the external magnetic field is removed, the nanoparticles do not agglomerate, facilitating their use in subsequent purification cycles and making them easier to handle.

Furthermore, the adsorption is also affected by the size of the nanoparticles. Various authors who have investigated this topic conclude that the number of adsorbed molecules per unit of mass of nanoparticles increases as their size decreases [62,63]. As the diameter of the nanoparticles decreases, their specific surface area increases, leading to a higher number of active sites available for the adsorption of molecules with which they come into contact [62].

Thus, the particle size in our samples could ensure the formation of more carboxylate groups during coating, thanks to their increased specific surface area, which in turn would increase the adsorption capacity of the nanoparticles.

#### 3.2.4. Thermogravimetric analysis



**Figure 4.** TGA curves of IONPs and IONPs@CA.

The TGA technique allows the evaluation of both the thermal stability and composition of materials, and it can be used to determine the amount of coating present on the surface of nanoparticles [64]. The curve of percentage mass loss as a function of temperature is depicted in Figure 4. For IONPs, the mass loss throughout the analysis interval was only 4.4%. This loss may be attributed to the evaporation of chemically and physically adsorbed water molecules [65]. IONPs@CA, on the other hand, exhibited a total mass loss of 13.6%. Up to 160 °C, the mass loss in this sample can be attributed to the evaporation of physically adsorbed water on the surface of the nanoparticles; the mass loss observed from 160 °C to approximately 350 °C may correspond to the decomposition of the citrate

coating the nanoparticle surface [47]. The difference between the mass loss percentages for each sample (13.6% for IONPs@CA and 4.4% for IONPs) can be used to estimate the percentage of citrate present in the coated nanoparticles, with this value being 9.2%. Previous studies report similar results [66,67].

### 3.2.5. Dynamic light scattering and zeta potential

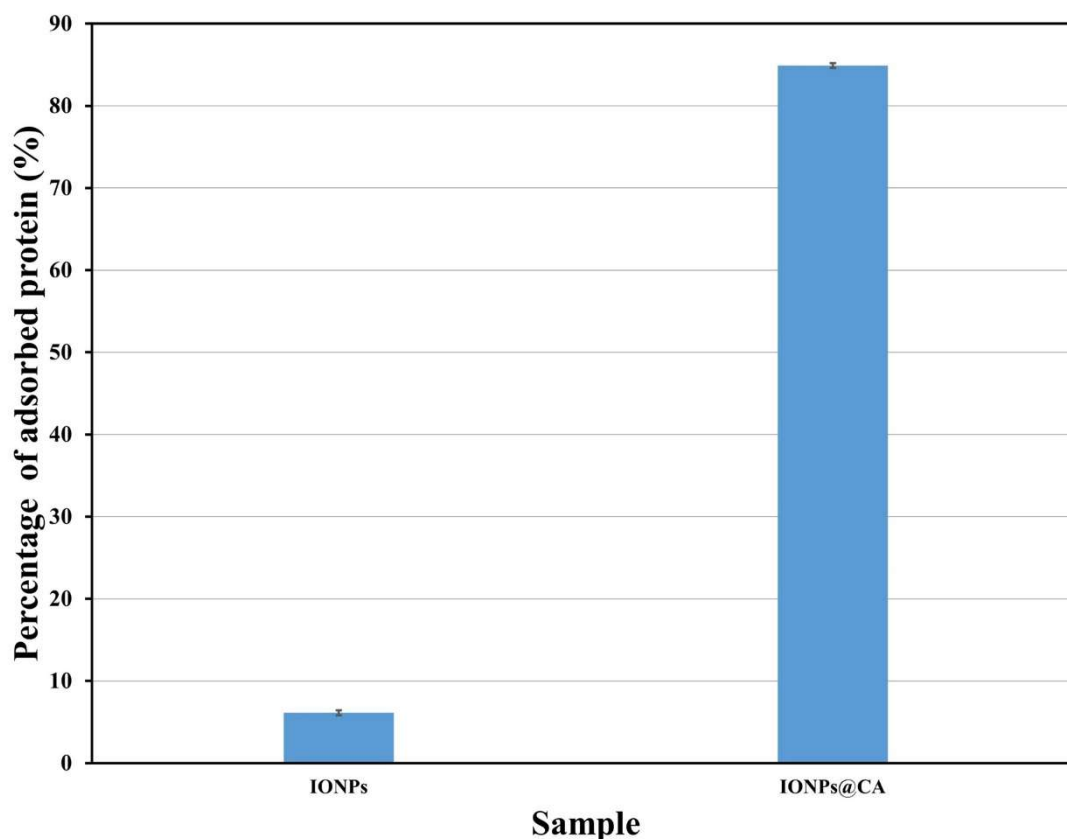
The DLS technique allows the determination of the hydrodynamic diameter of both individual particles and agglomerates of particles moving independently in a suspension [68]. The particle sizes obtained for the IONPs and IONPs@CA samples are shown in Table 2. The large difference between these results and the individual particle size (8 nm) suggests the formation of particle agglomerates in both samples, which can be confirmed by TEM images. Additionally, the table presents the values of the zeta potential for both samples. This parameter is widely used as an indicator of the colloidal stability of a suspension. A suspension with an absolute zeta potential value greater than 30 mV is considered highly stable [69], while suspensions with a zeta potential below this value tend to form agglomerates and flocculate due to Van der Waals forces causing particle attraction [70]. The zeta potential value for the IONPs sample was  $-28.90 \pm 0.52$  mV, while for IONPs@CA it was  $-31.65 \pm 0.57$  mV. This variation in the zeta potential value, after coating with citric acid, is consistent with previous research findings [71,72] and can be explained by the increase in negative charges on the surface of the nanoparticles caused by the presence of carboxylate groups. This increase in charges enhances the electrostatic repulsion between nanoparticles, reducing the tendency for aggregation and increasing the stability of the suspension [71]. In addition, the sign of the zeta potential (positive or negative) is often associated with the surface charge of the nanoparticles [73]. In our case, the nanoparticles have a negative zeta potential, which promotes interaction with lysozyme, as it is positively charged at pH 7.4 (the pH selected for the adsorption assays).

**Table 2.** Particle size according to DLS and Z potential (values are reported as mean  $\pm$  standard deviation).

Sample	D <sub>h</sub> (nm)	Z potential (mV)
IONPs	311 $\pm$ 21	-28.90 $\pm$ 1.65
IONPs@CA	482 $\pm$ 21	-31.65 $\pm$ 1.82
Lysozyme	-	+6.47 $\pm$ 0.83

### 3.3. Protein adsorption

The aim of this assay was to verify whether the presence of carboxylate groups (derived from the coating with citric acid) had any effect on the amount of protein adsorbed by the nanoparticles. Lyz was chosen for these tests as it is a protein with an isoelectric point in the range of 9.5–11.0 [74]; hence, at pH 7.4, it carries a positive charge, as shown in Table 2. After 4 h of interaction between the dissolved Lyz and the nanoparticles (IONPs and IONPs@CA), the percentage of adsorbed Lyz was determined for both samples, and the results are shown in Figure 5.

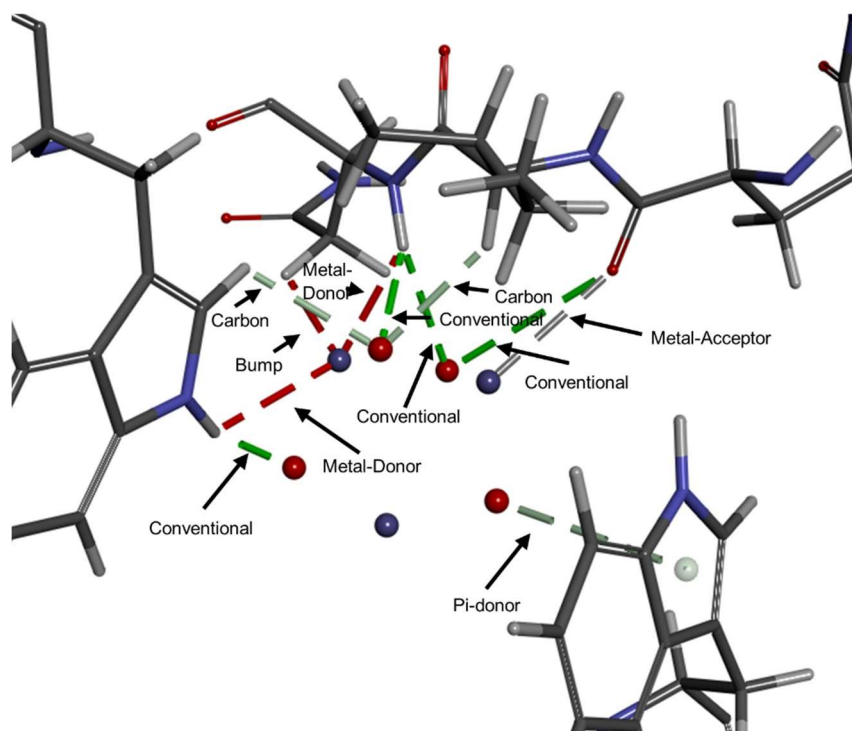


**Figure 5.** Percentage of protein adsorbed by nanoparticles.

The results demonstrate that both IONPs and IONPs@CA undergo Lyz adsorption, albeit to different extents. The adsorption yield for uncoated nanoparticles was  $6.1 \pm 0.3\%$ , while for coated nanoparticles, the yield was  $84.9 \pm 0.3\%$ . This difference can be attributed to the introduction of new functional groups on the nanoparticle surface, which increases the number of potential interaction sites between lysozyme and the nanoparticles.

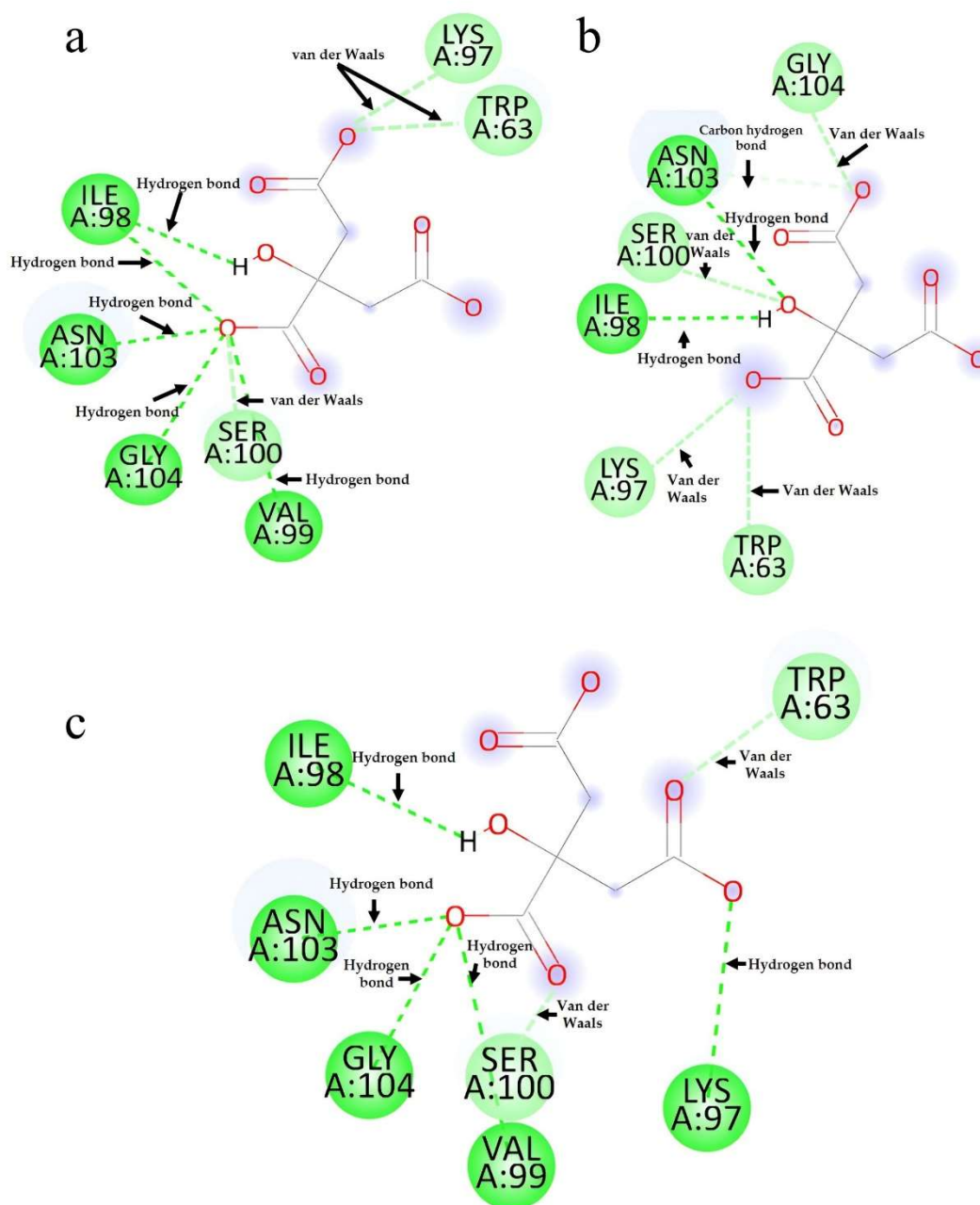
### 3.3.1. In silico evaluation by molecular docking

Molecular docking was conducted to analyze the mechanistic interactions of IONPs and IONPs@CA for binding with Lyz. Currently, molecular docking has garnered interest as a computational tool capable of predicting interactions and binding energies between ligands and target macromolecules, facilitating optimal binding selection [75]. The cubic structure of IONPs, confirmed via XDR analysis, is depicted in Figure 6. During in silico evaluation, 50 IONPs-Lyz and 50 citrate-Lyz dockings were obtained. Figure 6 (and Table S3) illustrates the most stable IONPs-Lyz docking, yielding a binding energy of  $-3.98$  kcal/mol and an inhibition constant of 1.21 mM. The primary amino acids of lysozyme involved in interactions with IONPs are asparagine (ASN), glutamine (GLN), and tryptophan (TRP). ASN binds to IONPs through conventional hydrogen bonds and metal-acceptor interactions. Similarly, GLN engages in metal-acceptor interactions, while TRP can act as an electron density donor due to the indole ring present in its structure. However, molecular docking results indicate that interactions such as bump and metal-donor may also occur between lysozyme and IONPs, potentially affecting the stability of the docking configuration [76,77].



**Figure 6.** IONPs and Lyz coupling.

Distinct outcomes were obtained from citrate-Lyz dockings, exhibiting varying binding energies and inhibition constants. Figure 7 displays the formation of predominantly stable bonds, compared to those formed with IONPs. We can highlight the potential hydrogen bonds that may form between isoleucine (ILE), valine (VAL), and lysine LYS with citrate; carbon-hydrogen bonds promoted by interactions with ASN at position 103 of lysozyme; and van der Waals interactions (involving TRP, serine (SER), and LYS), which collectively contribute to the increased stability of the binding. These results are comparable to those obtained by Vaidyanathan et al. (2023) in their study on the interactions between human serum albumin (HSA) and phenolic acid derivatives. The authors report interactions involving TRP, SER, and LYS with the  $-\text{COO}^-$  group [78]. Docking 19 (Figure 7a) yielded binding energy of  $-4.81$  kcal/mol, docking 11 of  $-4.56$  kcal/mol (Figure 7b), and docking 44 of  $-4.51$  kcal/mol (Figure 7c). Compared to the binding energy of IONPs docking, these values are significantly lower, indicating that Lyz exhibits greater affinity for IONPs@CA than IONPs [79]. Moreover, no unfavorable interactions were observed between citrate and the protein; this demonstrates the superior performance of IONPs@CA during lysozyme adsorption in comparison to IONPs.

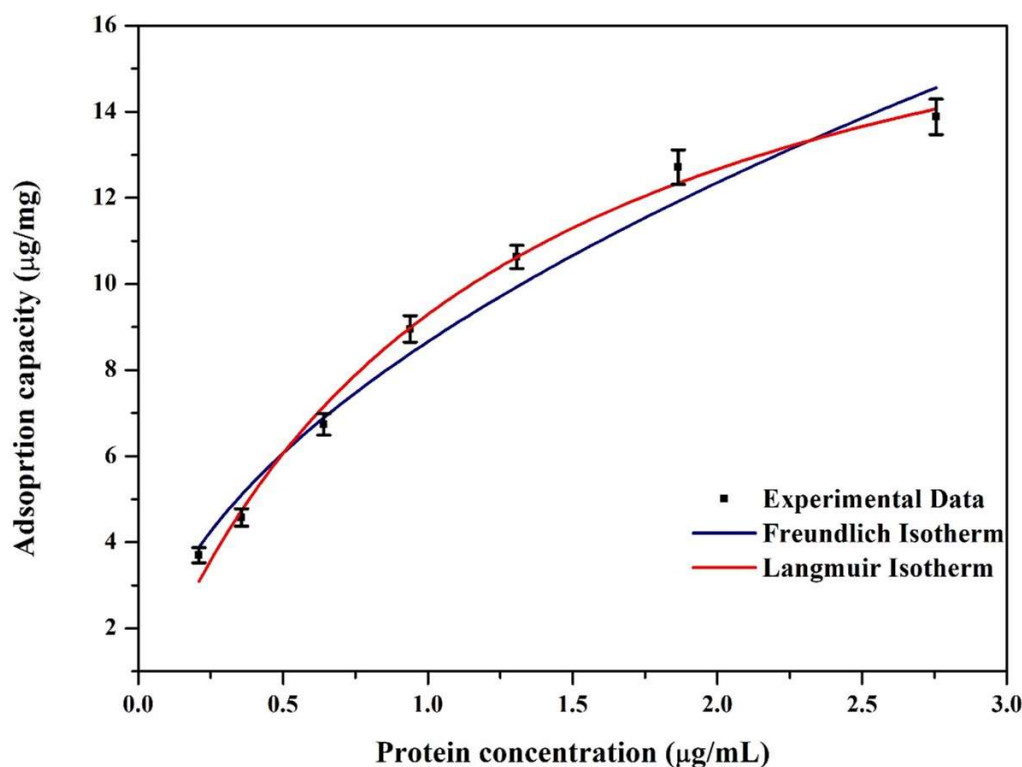


**Figure 7.** Citrate ion and Lyz coupling.

### 3.3.2. Adsorption isotherm

To determine the maximum adsorption capacity of coated nanoparticles, the adsorption isotherm was constructed. The graph of adsorption capacity (expressed in  $\mu\text{g}/\text{mg}$ ) as a function of protein concentration ( $\mu\text{g}/\text{mL}$ ) at equilibrium was fitted to the Langmuir [80] and Freundlich [81] adsorption models, respectively (see Figure 8). The statistical parameters  $R^2$  (coefficient of determination) and RMSE (root mean square error) were used to evaluate the quality of the fits, confirming that the Langmuir adsorption model best fits the experimental data (see Table 3). In contrast to these results, there are studies demonstrating that protein adsorption on solid surfaces does not comply with the

assumptions of the Langmuir isotherm model [82,83], but rather, it is a much more complex process. Despite this, and due to the simplicity of its mathematical expression (Eq 3), the model is still used to estimate data such as the maximum adsorption capacity of an adsorbent.



**Figure 8.** Fit of Lyz adsorption isotherm to Langmuir and Freundlich models.

**Table 3.** Estimated parameters of Langmuir and Freundlich models.

Isotherm model	Equation parameters			
	$q_m$ ( $\mu\text{g}/\text{mg}$ )	$K_L$ ( $\text{mL}/\text{mg}$ )	$R^2$	RSME
Langmuir model	$19.9 \pm 1.1^*$	0.88	0.99	0.35
Freundlich model	-	-	0.97	0.54

\*Standard error.

$$q_e = \frac{q_m \times K_L \times C_{eq}}{1 + K_L \times C_{eq}} \quad (3)$$

where  $q_e$  and  $q_m$  ( $\mu\text{g}/\text{mg}$ ) are the adsorption capacity of the adsorbent at equilibrium and the maximum adsorption capacity, respectively;  $K_L$  ( $\text{mL}/\mu\text{g}$ ) is the Langmuir constant relative to the adsorption capacity; and  $C_{eq}$  is the concentration of the adsorbate once adsorption equilibrium is reached. The adsorption capacity was calculated using the Eq 4:

$$\text{adsorption capacity} \left( \frac{\mu\text{g}}{\text{mg}} \right) = \frac{C_0 - C_f}{m_{np}} \times V \quad (4)$$

where  $C_0$  and  $C_f$  are the initial and final concentrations, respectively, of Lyz expressed in  $\mu\text{g/mL}$ ;  $m_{np}$  is the amount, expressed in mg, of nanoparticles added to the vial; and  $V$  is the volume, in mL, of the protein solution placed in the vial [34].

In this case, a maximum adsorption capacity of  $19.9 \mu\text{g}$  of protein per milligram of nanoparticles was achieved. Certainly, there are reports of nanoparticles, even without coating, used in protein adsorption, in which the amount of adsorbed protein was much higher than in our case [84–86]. However, the maximum initial protein concentration used for constructing our isotherm was  $23.6 \mu\text{g/mL}$ ; this value is considerably lower than those used in those reports ( $500$  [84],  $0.4$  [85],  $400 \text{ mg/mL}$  [86]). Regarding this, there is evidence that the adsorption capacity shows a direct dependence on the initial protein concentration [37,87,88], which could explain the relatively low value of the adsorption capacity of IONPs@CA when compared to previous research. In addition to concentration, there are other experimental factors that significantly influence the adsorption process, such as pH, ionic strength of the medium, and temperature [89]. The optimization of these parameters in our experiments could result in an increase in the adsorption capacity of the nanoparticles.

However, besides the maximum adsorption capacity, the percentage of adsorbed protein (see Eq 1) can be used to evaluate the performance of the nanoparticles. For this calculation, the Lyz solution with the highest concentration ( $23.6 \mu\text{g/mL}$ ) was used to estimate the maximum percentage of protein that could be adsorbed by IONPs@CA, which resulted in  $88.3\% \pm 0.2\%$ . Table 4 summarizes the performance of various molecules during the adsorption of lysozyme. As observed, citric acid has an efficiency of  $88.3\%$ , making it a very competitive adsorbent agent, outperforming succinic anhydride [90] and  $\beta$ -glucosidase [91].

**Table 4.** Adsorption efficiency using different coatings.

Coating agent	Adsorption efficiency	Reference
Succinic anhydride	62%	[90]
<sup>1</sup> LMW-polyacrylic acid	98%	[90]
<sup>2</sup> HMW-polyacrylic acid	100%	[90]
$\beta$ -glucosidase	80%	[91]

1: Low molecular weight; 2: high molecular weight.

#### 4. Conclusions

IONPs were successfully synthesized with a crystalline structure consistent with magnetite and maghemite phases of iron oxide using the coprecipitation method. These nanoparticles, with an average particle size of  $8 \text{ nm}$ , were further modified with citric acid, as confirmed by FT-IR spectroscopy and dynamic light scattering. The addition of new functional groups on the nanoparticle surface enhanced the colloidal stability of the material, indicated by the more negative Z potential values for the IONPs@AC compared to the uncoated nanoparticles. The hypothesis that the coating could improve the adsorption of Lyz onto nanoparticles was confirmed in *in silico* studies, achieving a maximum adsorption percentage of  $88.3\%$  after the surface modification of the nanoparticles. This underscores the effectiveness of surface modification in improving the adsorption capacity of the nanoparticles, which has significant implications for various biomedical and environmental applications.

## Use of AI tools declaration

The authors declare they have not used Artificial Intelligence (AI) tools in the creation of this article.

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Conceptualization: H. Y. M., R. M. E, D. A. P, A. A. V. L.; methodology: D. A. P and A. A. V. L; software: A. A. V. L.; validation: H. Y. M. and R. M. E.; formal analysis: D. A. P.; investigation: D. A. P.; resources: H. Y. M.; data curation: D. A. P. and A. A. V. L.; writing original draft preparation: D. A. P. and A. A. V. L; writing, review and editing: H. Y. M. and R. M. E.; supervision: R. M. E. and H. Y. M.; project administration: H. Y. M. and R. M. E.; funding acquisition: H. Y. M. and R. M. E. All authors have read and agreed to the published version of the manuscript.

## Conflict of interest

The authors declare no conflict of interest.

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